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EEG Artifact Removal Strategies for BCI Applications: A Survey

Pardhu Thottempudi¹, Vijay Kumar², Nagesh Deevi¹

1- Department of Electronics and Communications Engineering, BVRIT HYDERABAD College of Engineering for Women, Hyderabad, India.

Email: Pardhu.t@bvrithyderabad.edu.in (Corresponding author) , nagesh.d@bvrithyderabad.edu.in 2- School of Electronics Engineering (SENSE), Vellore Institute of Technology, Vellore, India. Email:vijaykumar@vit.ac.in

ABSTRACT:

This paper aims to provide a comprehensive examination of the Brain-Computer Interface and the more scientific discoveries that have resulted from it. The ultimate goal of this review is to provide extensive research in BCI systems while also focusing on artifact removal techniques or methods that have recently been used in BCI and important aspects of BCIs. In its pre-processing, artifact removal methodologies were critical. Furthermore, the review emphasizes the applicability, practical challenges, and outcomes associated with BCI advancements. This has the potential to accelerate future progress in this field. This critical evaluation examines the current state of BCI technology as well as recent advancements. It also identifies various BCI technology application areas. This detailed study shows that, while progress is being made, significant challenges remain for user advancement A comparison of EEG artifact removal methods in BCI was done, and their usefulness in real-world EEG-BCI applications was talked about. Some directions and suggestions for future research in this area were also made based on the results of the review and the existing artifact removal methods.

KEYWORDS: EEG, BCI, ECG, EMG, EOG.

1. INTRODUCTION

1.1. Signal Capturing Block

The electrophysiological signals used by the BCI are captured by the Signal Capturing Module. The brain is the source of these signals [7]. Both invasive and non-invasive methods have been developed for BCI research, but invasive methods like electrocardiograms (ECoG) and single-neuron recordings have proven more effective [7,8]. Comparison of signal quality with other non-invasive brain imaging techniques, including magnetoencephalography, positron emission tomography, functional magnetic resonance imaging, near-infrared spectroscopy, and fMRI [8]. The acquired signals are amplified to increase their strength before transmission. Before any computer application, they must be encoded.

1.2. Signal Capturing Block

As illustrated in Fig. 1, preprocessing of EEG signals is an essential first step in any brain-computer interface-based application. The signal is cleaned up by subtracting out artifacts like ECG, EOG, and EMG measurements, filtering out noise, and resampling it to meet detector input specifications.

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Fig. 1. Stage of the Signal Processing in BCI.

Pre-processing is often done to increase the recorded data's signal to noise ratio before processing. Artifacts in the EEG signal can be eliminated by filtering out the electrical activity produced by head and eye muscle contractions. In order to remove artifacts from an EEG recording, a preprocessing of the signal is required. When properly implemented, BCI systems can Accurate categorization relies heavily on the EEG signal being properly preprocessed. The EEG signal can be cleaned up and made ready for analysis by doing some preliminary processing. BSS, which stands for "blind source separation," is a popular pre-processing method [9].Artifacts are frequently observed in many forms of EEG signals, as shown in Table 1.

Table 1. Different artifacts arised during signal acquisition of EEG signal processing.

| S.No | Artifacts | Generated By The Source | Frequency | Voltage | Shape /Structure |
|------|-------------------|------------------------------|-------------|-----------|-----------------------|
| | | | | Level | |
| 1 | Ocular | Eye | 0.3 -3HZ | 80-100mv | Delta waves |
| | Artifacts (EOG) | | | | |
| 2 | EMG | Jaw movements | 4-6hz | 0-10mv | Theta waves |
| 3 | ECG | Heart or cardiac movement | 0-150hz | 1-10mv | Beta and gamma |
| | | | | | waves |
| 4 | 50/60 HZ | Power line attached | 50/60 hz | high | Beta and gamma |
| | artifacts(power | | | | waves |
| | line artifacts) | | | | |
| 5 | Sweat artifacts | sweat | 0.25-0.5 hz | 300 micro | Delta waves |
| | | | | volts | |
| 6 | Electrode pop | Electrodes attached to scalp | 0-30hz | 20 mv | Shape appeared |
| | | | | | different from actual |
| | | | | | EEG signal |
| 7 | Physical | Body movements,head | Very low | high | Shape appeared |
| | movement | movement, jaw movement etc | | | different from actual |
| | artifacts(motion | | | | EEG signal |
| | artifacts) | | | | |
| 8 | Electronic | Mobile, laptop, personal | Very low | high | Shape appeared |
| | gadgets artifacts | computer etc | | | different from actual |
| | | | | | EEG signal |

2. LITERATURE REVIEW

The below Table.2 compare the latest artifacts removal techniques in various parameters such as type of artifacts that can able to eliminate in EEG signal processing which is mainly related to BCI applications ,novelty in the algorithm or method that chosen to mitigate artifacts ,the data that can operated on which the proposed method can best suited (real &simulated) so that we can estimate practical implementation, and also here discussed the challenges or limitations faced to practical viability and commented or given remarks about each and every system of implementation. The above table contain different artifacts removal techniques EOG, ECG, EMG, Physical movement artifacts(motion artifacts) etc but mainly focused on ocular or Eye Blink (EB) artifacts because the EB artifacts are main cause of error or distortion in EEG signal pre-processing.

| Author | Type | Method | Algorithm | Novelty | Data | Challenges/ | Comment |
|----------------|-------------|-----------------|-----------------|-----------------|------------|-------------------|----------------|
| | of artifact | | used | | | limitations | s |
| Çınar, | Only | Independent | The classical | The | Real | It is only | The |
| Salim(2021)[22 | Eye blink | Component | Least Mean | proposed | &simulated | applicable to | proposed |
| 1 | (EOG) | Analysis (ICA), | Squares (LMS) | system does | | this method is | method has |
| - | | Kurtosis, K- | and | require an | | that ocular | high |
| | | means, Modified | Normalized | external | | artifacts and | performance |
| | | Z-Score (MZS) | LMS (NLMS) | electrode for | | other artifacts | in both |
| | | and Adaptive | algorithms | measuring | | present it is not | datasets & |
| | | Noise Canceller | _ | EOG Signals | | efficient | comfortable |
| | | (ANC). | | | | method and | measurement |
| | | | | | | When | for patients |
| | | | | | | conducting the | during more |
| | | | | | | subtraction | time EEG |
| | | | | | | process, the | recordings. |
| | | | | | | disadvantage is | |
| | | | | | | the relevant | |
| | | | | | | EEG signals | |
| | | | | | | can be erased. | |
| Cao, | Only | Gaussian | cascaded | No false | Real and | An | In terms |
| Jiuwen.et al. | Eye blink | mixture model | hybrid | positives were | simulated | increased | of precision |
| (2021) [24] | (EOG | (GMM) | thresholding | found in the | | likelihood of | and F1 score, |
| | | | method and the | detection of | | missing | the proposed |
| | | | GMM | eye blink | | artifacts caused | approach is |
| | | | algorithm | artifacts using | | by eye blinks | more |
| | | | | the suggested | | when | reliable. |
| | | | | approach. | | employing a | |
| | | | | | | high threshold. | |
| Egambaram | Only | FastEMD- | It is | More than | simulate | The | Eyeblink |
| , | Eye blink | CCA and | proposed to use | 97% Removal | d | artifact-free | artifacts can |
| Ashvaany.etal. | (EOG | FastCCA | a combination | Accuracy and | | EEG samples | be effectively |
| [26] | | | of modified | an average of | | showed | removed |
| | | | Empirical | 10-13ms | | negligible | online with |
| | | | Mode | removal speed | | variation. | mınımal |
| | | | Decomposition | | | | neural |
| | | | and Canonical | | | | distortion. |
| | | | Correlation | | | | |
| | | | Analysis to | | | | |
| | | | perform | | | | |
| | | | unsupervised | | | | |
| | | | eye blink | | | | |
| | | | artifiact | | | | |
| | | | | | | | |
| | 1 | 1 | (CADA). | 1 | | | 1 |

| Table 2. | Comp | arison | of variou | s artifacts | remov | val techniq | ue | s |
|----------|------|--------|-----------|-------------|-------|-------------|----|---|
| | | | | | | | | |

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| Borowicz, | Only | independent | multichann | When | Real and | utilizing | When |
|----------------------|--------------------|-------------------|-------------------------------|------------------------|-----------|----------------------------|----------------------|
| Adam. [27] | Eye blink | component | el Wiener filter | compared to | simulated | cutting-edge | compared to |
| | (EOG | analysis (ICA) | (MWF) and a | the ICA | | multichannel | the state-of- |
| | | and principles of | small subset of | approach, the | | linear filters, | the-art |
| | | regression | the frontal | suggested | | enhanced off- | method, the |
| | | analysis | electrodes | algorithm is | | line | new |
| | | | | more straightforwar | | implementatio | is more |
| | | | | d Real-time | | expanding the | suitable to |
| | | | | systems can | | suggested | real-time |
| | | | | benefit more | | method's | systems. |
| | | | | from it, and | | applicability to | - |
| | | | | that seems to | | additional | |
| | | | | be a crucial | | types of | |
| | | | | factor in BCI | | biomedical | |
| | | | | research and | | data. | |
| | 0.1 | | T 1 1 | development. | D 1 1 | | |
| Zhou, Weideng and | Only Even blimb | ICA method | Independen t Common an ant | The ICA | Real and | The | This method |
| Jean Gotman | Eye olink | | Analysis (ICA) | few | simulated | distributions of | was validated for |
| [28] | | | combining | computational | | slow waves and | its ability to |
| [=0] | | | the EEG dipole | resources. | | visual artifacts | automatically |
| | | | model | Without | | are very | filter out |
| | | | | requiring | | similar. | EEG |
| | | | | access to a | | | aberrations |
| | | | | database of | | | attributable |
| | | | | reference | | | to the eyes. |
| | | | | artifacts, it can | | | |
| | | | | FEG from the | | | |
| | | | | noise | | | |
| | | | | 110150 | | | |
| . Sreeja, S. | Mainl | morphologic | MCA and K- | The | Real and | One major | It is |
| R., et al [29] | y Eye | al component | SVD are two | suggested | simulated | drawback is | applicable to |
| | blink | analysis (MCA) | sparsity-based | sparsity-based | | that it | the |
| | (EOG) & | and K-SVD | approaches that | approaches can | | necessitates the | elimination |
| | also used | | can be used to | eliminate EB | | use of | of other |
| | for other | | artifacts | EFG signal | | extraocular channels in | artifiacts in FEG |
| | removal | | artifacts. | without the use | | order to capture | data as well |
| | 1 51110 V UI | | | of anv | | ocular artifacts. | aata ab won. |
| | | | | specialized | | | |
| | | | | equipment or | | | |
| | | | | additional | | | |
| | | | | channels for | | | |
| | | | | the EOG. | | | |
| He, Ping, G. | ocular | adaptive | recursive | The non- | real | The | automatically |
| Wilson, and C. | artifacts | nitering | least squares | stationary | | approach does | adjust to a |
| Russen [30] | | | argonulli | FOG signals is | | situations with | new environment |
| | | | | monitored | | four or more | without |
| | | | | using this | | reference | sacrificing |
| | | | | technique. | | inputs. | performance |
| | | | | | | | |

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| . Chintala, | ocular | Robust | RVFF-RLS | The non- | Real and | Non- | The |
|--|--|--|---|--|---------------------|--|--|
| Sridhar, and | artifacts | Variable | based | stationary | simulated | stationary | proposed |
| Jaisingh | | Forgetting | algorithm | EOG signals | | conditions are | method |
| Thangaraj[32] | | Factor (RVFF) | | are followed | | detrimental to | exhibits the |
| | | and Recursive | | and estimated | | tracking | lowest |
| | | Least Square | | by the | | performance. | possible |
| | | (RLS) | | algorithm, and | | 1 | mean square |
| | | | | then the | | | error in a |
| | | | | subtraction | | | time-varving |
| | | | | approach is | | | condition |
| | | | | used to acquire | | | condition. |
| | | | | clean FEG | | | |
| | | | | data | | | |
| 37 1 | 1 | | E 11 | uaia. | | | D |
| Yadav, | ocular | EEMD & | Ensemble | To counter | Real | EEMD's | Better |
| Anchal, and | artifacts | SCICA | Empirical | act EMD's | | amplitude- | constraints |
| Mahipal Singh | | Kurtosis and | Mode | mode mixing | | reduction | on ICA and |
| Choudhry. [33] | | mMSE | Decomposition | and aliasing, | | problem | wavelet |
| | | | (EEMD) and | EEMD is | | | augmented |
| | | | Spatial | employed. | | | independent |
| | | | Constraint | | | | component |
| | | | Independent | | | | analysis can |
| | | | Component | | | | boost |
| | | | Analysis | | | | performance |
| | | | (SCICA) | | | | even further. |
| | | | () | | | | |
| Gaibhiya | ocular | the FRSE EWT | The | The approach | Peol | The | Compared to |
| Dramiali Daiaah | oculai | head where there | . Ille Equinion Descel | | Keal | hlanding of | compared to |
| Pranjan, Kajesn | artifacts | based mythm | гоипет-bessei | | | | existing |
| Kumar | | separation | series | ocular artifact | | modes as | methods, the |
| Tripathy [34] | | technique | expansion | from an EEG | | various | proposed |
| | | | | | | whythman LL() | |
| | | | based empirical | recording | | inyunne EEG | approacn |
| | | | wavelet | without the | | data appears | approach improves |
| | | | wavelet transform | without the use of a | | data appears | approacn improves performance |
| | | | wavelet transform (FBSEEWT | without the use of a reference | | data appears | approacn improves performance while |
| | | | wavelet transform (FBSEEWT | without the use of a reference signal. | | data appears | approach improves performance while requiring |
| | | | wavelet transform (FBSEEWT | without the use of a reference signal. | | data appears | approacn improves performance while requiring fewer |
| | | | wavelet transform (FBSEEWT | without the use of a reference signal. | | data appears | approacn improves performance while requiring fewer resources. |
| | | | wavelet transform (FBSEEWT | without the use of a reference signal. | | data appears | approacn improves performance while requiring fewer resources. When |
| | | | wavelet transform (FBSEEWT | without the use of a reference signal. | | data appears | approacn improves performance while requiring fewer resources. When compared to |
| | | | wavelet transform (FBSEEWT | without the use of a reference signal. | | data appears | approacn improves performance while requiring fewer resources. When compared to other |
| | | | wavelet transform (FBSEEWT | without the use of a reference signal. | | data appears | approacn improves performance while requiring fewer resources. When compared to other methods. |
| | | | wavelet transform (FBSEEWT | without the use of a reference signal. | | data appears | approacn improves performance while requiring fewer resources. When compared to other methods, alpha wave's |
| | | | wavelet transform (FBSEEWT | without the use of a reference signal. | | data appears | approacn improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD |
| | | | wavelet transform (FBSEEWT | without the use of a reference signal. | | data appears | approacn improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was |
| | | | wavelet transform (FBSEEWT | without the use of a reference signal. | | data appears | approacn improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on |
| | | | wavelet transform (FBSEEWT | without the use of a reference signal. | | data appears | approacn improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average |
| | | | wavelet transform (FBSEEWT | without the use of a reference signal. | | data appears | approacn improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average. |
| Islam, Md | All type | Entropy, | stationary | The outcomes | Real & | The . | approacn improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average. The |
| Islam, Md Kafiul, Parviz | All type of | Entropy, kurtosis, | stationary wavelet | The outcomes demonstrate | Real & simulated | The proposed | approacn improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average. The proposed |
| Islam, Md Kafiul, Parviz Ghorbanzadeh, | All type of artifacts | Entropy, kurtosis, skewness, | stationary wavelet transform (FBSEEWT stationary | The outcomes demonstrate that the | Real & simulated | The proposed method still | approacn improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average. The proposed approach |
| Islam, Md Kafiul, Parviz Ghorbanzadeh, and Amir | All type of artifacts removal(| Entropy, kurtosis, skewness, periodic | stationary wavelet transform (FBSEEWT stationary wavelet transform based artifact | The outcomes demonstrate that the suggested | Real & simulated | The proposed method still requires work | approacn improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average. The proposed approach utilizes four |
| Islam, Md Kafiul, Parviz Ghorbanzadeh, and Amir Rastegarnia. | All type of artifacts removal(ECG, | Entropy, kurtosis, skewness, periodic waveform index | stationary wavelet transform (FBSEEWT stationary wavelet transform based artifact removal | The outcomes demonstrate that the suggested reduction of | Real & simulated | The proposed method still requires work in terms of its | approacn improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average. The proposed approach utilizes four statistical |
| Islam, Md Kafiul, Parviz Ghorbanzadeh, and Amir Rastegarnia. [35] | All type of artifacts removal(ECG, EOG, | Entropy, kurtosis, skewness, periodic waveform index | stationary wavelet transform (FBSEEWT stationary wavelet transform based artifact removal | The outcomes demonstrate that the suggested reduction of artifacts | Real & simulated | The proposed method still requires work in terms of its discrimination | approacn improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average. The proposed approach utilizes four statistical techniques to |
| Islam, Md Kafiul, Parviz Ghorbanzadeh, and Amir Rastegarnia. [35] | All type of artifacts removal(ECG, EOG, EMG, | Entropy, kurtosis, skewness, periodic waveform index | stationary wavelet transform (FBSEEWT stationary wavelet transform based artifact removal | The outcomes demonstrate that the suggested reduction of artifacts significantly | Real & simulated | The proposed method still requires work in terms of its discrimination abilities and its | approacn improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average. The proposed approach utilizes four statistical techniques to plot the |
| Islam, Md Kafiul, Parviz Ghorbanzadeh, and Amir Rastegarnia. [35] | All type of artifacts removal(ECG, EOG, EMG, etc.) | Entropy, kurtosis, skewness, periodic waveform index | stationary wavelet transform (FBSEEWT stationary wavelet transform based artifact removal | The outcomes demonstrate that the suggested reduction of artifacts significantly increases BCI | Real & simulated | The proposed method still requires work in terms of its discrimination abilities and its capacity to | approacn improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average. The proposed approach utilizes four statistical techniques to plot the improbability |
| Islam, Md Kafiul, Parviz Ghorbanzadeh, and Amir Rastegarnia. [35] | All type of artifacts removal(ECG, EOG, EMG, etc.) | Entropy, kurtosis, skewness, periodic waveform index | stationary wavelet transform (FBSEEWT stationary wavelet transform based artifact removal | The outcomes demonstrate that the suggested reduction of artifacts significantly increases BCI output. | Real & simulated | The proposed method still requires work in terms of its discrimination abilities and its capacity to eliminate | approacn improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average. The proposed approach utilizes four statistical techniques to plot the improbability of various |

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| τ | M | | | E | D1 0 | т: | Developed |
|----------------|-------------|---------------|-----------------|--------------------|-----------|-----------------|-------------------|
| Lee, | wovemen | | constrained | Examining the | | | Developed a |
| Young-Eun, | t artifacts | learning | independent | impact of | simulated | for using the | rough |
| No-Sang | | | component | noise | | approach are | estimate of |
| Kwak, and | | | analysis with | reduction in | | constrained by | the |
| Seong-Whan | | | online learning | the temporal | | the occurrence | movement |
| Lee [36] | | | (cIOL) | and frequency | | of gait | artifacts |
| | | | | domains | | events. Anothe | using the |
| | | | | through a | | r issue is that | EEG data. |
| | | | | quantitative | | there isn't a | Finally, |
| | | | | evaluation of | | single adequate | artifact-free |
| | | | | artifact | | template to | EEG signals |
| | | | | removal | | represent | were |
| | | | | approaches | | artifacts' wide | recovered |
| | | | | utilizing two | | variety. | using |
| | | | | BCI naradioms | | | weights that |
| | | | | (ERP and | | | were updated |
| | | | | (EIG and SSVEP) | | | using online |
| | | | | 55 v L1 <i>)</i> . | | | learning |
| | | | | | | | icarining. |
| Song. | EMG | ICA. PCA. and | EMG-CCh | Reduce | simulate | Methodologica | Finally, the |
| YoungJae, and | artifacts | BSS-CCA | Line con | ambiguity and | d | l Constraints | proposed |
| Francisco | | 222 0011 | | enhance | - | An excessive | strategy |
| Sepulveda [37] | | | | discrimination | | amount of | improved |
| Separieda [57] | | | | hetween | | class- | class |
| | | | | classes | | dependent | senaration |
| | | | | C1035C3. | | EMG can | (when |
| | | | | | | nersist even in | compared to |
| | | | | | | a channel with | prior |
| | | | | | | a channel with | prior mathada) |
| | | | | | | leauced CRC | |
| | | | | | | | |
| | | | | | | conditions. | training and |
| | | | | | | | test data. |
| | | | | | | | The data set |
| | | | | | | | developed |
| | | | | | | | for the BCI |
| | | | | | | | competition |
| | | | | | | | is used in a |
| | | | | | | | wide variety |
| | | | | | | | of |
| | | | | | | | applications. |
| | | | | | | | This strategy |
| | | | | | | | can be used |
| | | | | | | | independentl |
| | | | | | | | y or in |
| | | | | | | | tandem with |
| | | | | | | | other |
| | | | | | | | approaches |
| | | | | | | | of managing |
| | | | | | | | artifacts |
| | | | | | | | |

According to the data in the table above, the most common techniques used to clean up EEG signals include Blind Source Separation (BSS), Principal Component Analysis (PCA), Canonical Correlation Analysis (CCA), Discrete Wavelet Transform (DWT), Stationary Wavelet Transform (SWT), Empirical Mode Decomposition (EMD), Ensemble Empirical Mode Decomposition (EEMD), Wavelet Transform, and Adaptive Filtering. The performance parameters,

including the correlation co-efficient, Mean Square Error, Power Spectral Density, Signal-to-Noise Ratio, and Execution Speed and Complexity, are all improved when the preprocessing stage is enhanced.

The above table details a discussion of advanced artifact removal techniques for the examples given, including those by nar, Salim(2021), who discussed and implemented a new algorithm, the classical Least Mean Squares (LMS) algorithm, and the Normalized LMS algorithm (using Independent Component Analysis, Kurtosis, K-means, a modified Z-score, and an adaptive noise canceler) for removing eye blink artifacts from both real and simulated data. The system has the limitation of only being able to deal with ocular artifacts, making it a less-than-efficient method; the subtraction process can result in the loss of important EEG signals; and in another paper by Borowicz and Adam, they discussed independent component analysis (ICA) and regression analysis principles and implemented them using a multichannel Wiener filter; and in this study, they used a subset of frontal electrodes to detect ICA. It also works great with real-time systems, which is apparently crucial for BCI research. Additionally, a novel concept was implemented by Zhou, Weidong, and Jean Gotman using Independent Component Analysis in combination with the EEG dipole model, with a primary focus on ocular artifact elimination. This technique was found to be effective in automatically eradicating ocular artifacts from the EEG. Song, YoungJae, and Francisco Sepulveda also implemented the system using ICA, in addition to PCA, and BSS-CCA to remove EMG artifacts by a novel technique called EMG-cch and best suited for use along with the other techniques the data only implemented on simulation results.

Genetic algorithm (GA), a technique proposed by Trigui, Omar, et al., decreases the RMSE between unprocessed and processed EEG data. Using only simulated data and a small number of channels, the proposed approach nevertheless achieves satisfactory results.

Each and every eye blink artifact was correctly identified by the proposed method by Cao, Jiuwen.etal, with zero false positives.

The method developed by Egambaram, Ashvaany, et al. CFast EMD-CCA and Fast CCA introduced a method for detecting eye blink artifacts without human supervision by combining a variant of Empirical Mode Decomposition with Canonical Correlation Analysis. Artifact-free EEG segments showed hardly any distortion, with an accuracy of more than 97% and a removal speed of 10-13 ms, on average. Artifacts caused by an eyeblink can be corrected online with minimal neural distortion.

To eliminate EB artifacts from the EEG signal, Sreeja, S. R., et al. suggested a method known as K-SVD with morphological component analysis. Both of these methods are sparsity-based methodologies that work on both real and simulated data without the need for channel information, parameter tweaking (such as thresholding), or additional hardware/EEG channels.

Adaptive filtering for ocular artifacts using recursive least squares was given by He, Ping, G. Wilson, and C. Russell. When applied to real-world data, this method follows the dynamic components of EOG signals. It cannot be generalized to situations involving three or more reference inputs, but it can be automatically adapted to a new setting without compromising its efficacy.

Using the Robust Variable Forgetting Factor (RVFF) and Recursive Least Square (RLS), Chintala, Sridhar, and Jaisingh Thangaraj solved the problem of ocular artifacts. This method estimates and follows non-stationary EOG signals so that pure EEG signals can be extracted from both real and simulated data. In unstable conditions, tracking accuracy decreases. The proposed method achieves the smallest mean square error in a dynamic environment.

Yadav, Anchal, and Mahipal Singh Choudhry compute Kurtosis and mean squared error (mSSE) using Ensemble Empirical Mode Decomposition (EEMD) and Spatial Constraint Independent Component Analysis (SCICA). EEMD is also used to overcome the mode mixing and aliasing problem of EMD, which is typically performed on Real data. Improving the constraints used in ICA and wavelet-enhanced independent component analysis can further boost performance. In order to get rid of ocular artifacts, Gajbhiye, Pranjali, and Rajesh Kumar Tripathy presented a rhythm separation technique based on FBSE-EWT. Ocular artifacts can be removed from an EEG signal using the Fourier-Bessel series expansion based empirical wavelet transform (FBSEEWT) method, which has been extensively validated for real-valued data and does not require a reference signal. When many modes of EEG rhythm information appear, this phenomenon is referred to as "mode mixing." The suggested method outperforms state-of-the-art alternatives, with a mean absolute error (MAE) in peak signal-to-noise ratio (PSR) of only 0.029 for rhythm.

Using entropy, kurtosis, skewness, and the stationary wavelet transform, Islam, Md. Kafiul, Parviz Ghorbanzadeh, and Amir Rastegarnia proposed a method for eliminating artifacts across all modalities. When evaluated with real and simulated data, the results reveal that the proposed artefact removal significantly improves BCI output. The proposed technique still needs better discrimination capacity and has weak ability to eliminate genuine artefacts. The suggested method for mapping artificial probability uses four statistical parameters.

3. CONCLUSION

The work is mostly considered in the preprocessing step of the overall BCI systems. The goal of the pre-processing

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stage in a BCI applications is to decrease artifacts in the EEG signal generated by the numerous sources. Based on the findings in the available literature, this report summarized the key techniques, Some of the techniques uses exclusively used for removing artifacts which is related to eye blink (EOG)artifacts, ECG ,EMG and all other movement related artifacts here by go through the different research articles basically uses different algorithams separately or combinely that reveals the output without artifacts in EEG signal processing which combined with BCI related applications either it may be cursor movement,wheel chair movement,video gaming,bio medical etc. Some methods, such as adaptive filtering, Morphological Component Analysis (MCA) and K-SVD and Entropy, kurtosis, skewness, periodic waveform index, remove artifacts with high precision, which works on both real and simulated data or either of the one , however methods with high computational cost may not be suited for online applications. As a result, there is no best option for removing all forms of artifacts. So, one of the future goals of effective artifact attenuation is to provide an application-specific methodology with improved time and precision, efficiency.

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